

Power Spectral Changes of Quantitative EEG in the Subjective Cognitive Decline: Comparison of Community Normal Control Groups

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Purpose: The purpose of this study is to compare and analyze the power spectral changes between subjective cognitive decline (SCD) subjects and normal controls (NC) while checking the preclinical stage of AD in the SCD subjects and to use the derived data for biomarker research that can diagnose early-stage AD in the future.

Methods: We recruited 23 SCD patients and 23 normal control subjects and QEEG analysis including power spectral density (PSD) and source-level analysis were performed. An automated preprocessing procedure and statistical analysis were performed by iSync Brain[®] (iMediSync Inc., Republic of Korea) (<https://isyncbrain.com/>) using the international standard 10–20 system (19 electrodes).

Results: Absolute PSD, there was no statistically significant difference in all of the EEG power measurements of the 19 channels. In the relative PSD analysis, the average delta band power of the SCD group was significantly higher in Fp2, F4, and F8 than NC. Alpha1 band power of the O1 channel was 22.56 ± 16.05 for the SCD group and 33.19 ± 19.05 for the NC (p -value < 0.05). Source-level analysis did not show a statistically significant difference.

Conclusion: SCD subjects showed a partial increase of delta waves in the frontal lobe region and a partial decrease in alpha1, a fast wave in the occipital region, compared to the NC. SCD is considered one of the earliest clinical symptoms of AD and it is predicted to be related to minor nerve damage. We were able to observe the power spectral changes in SCD subjects in this cross-sectional study, a large number of subjects and longitudinal studies are needed to evaluate their predictability for future deterioration such as conversion to MCI.

Keywords: Alzheimer, cognitive impairment, dementia, hypertension

Introduction

Subjective cognitive decline (SCD) is defined normally by standardized neuropsychological tests, but there is often a self-perception of worsening or more frequent confusion or memory loss for the individual.¹ An aging society where diversification and complexity coexist is increasing the frequency of humans experiencing forgetfulness. Nowadays, people are increasingly aware that the main symptom of dementia is a problem related to memory, so the number of patients visiting hospitals is increasing and the rate of concern over SCD is also increasing.^{2–4}

SCD was first described for the evaluation of degenerative dementia in 1982, and has been referred to as various expressions such as subjective cognitive impairment, subjective memory impairment, subjective memory decline, and subjective memory failure. In standardized neuropsychological tests, SCD is characterized by normal

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performance unlike Mild Cognitive Impairment (MCI), but the optimal approach, such as having standardized criteria for diagnosis, has hardly been known. However, the number of cases that appear as the first progenitor symptom in Alzheimer's disease (AD) has been increasing recently, and that is receiving great attention from academia and in clinical practice.^{1,5-9}

In previous studies on SCD, low hippocampal volume, brain structural changes such as white matter changes, reduction in memory of future plans, and the presence or absence of apolipoprotein E (APOE) $\epsilon 4$ were reported to be associated with SCD.¹⁰⁻¹³ However, it is true that standardized criteria or biomarkers for discriminating SCD diagnosis, such as results due to emotional changes such as depression or anxiety disorders, are still insufficient.^{14,15}

The conventional electroencephalography (EEG) test is a biological marker of brain function, and unlike other imaging tests, it has excellent temporal resolution, is non-invasive, is easy to measure, and is economical. However, it has difficulty diagnosing cognitive dysfunction and neurodegenerative diseases due to lack of objectivity because it relies only on the visual judgment of an EEG expert. These shortcomings have been supplemented by techniques such as extracting specific parameters by analyzing data of continuous variables with Quantitative EEG (QEEG), and now, studies on evaluating brain function, and early diagnosis of degenerative brain disorders, such as AD and AD-MCI are actively progressing.¹⁶⁻¹⁸ Power spectrum, which is one method in the analysis of QEEG signals, is a well-established core part of a general method used in clinical research. The most frequently observed spectral change so far is presumed to be related to the degree of cognitive decline due to the increase in the slow wave of EEG.^{19,20} However, little is known about the change in the power spectrum of SCD, which is thought to be the earliest stage of cognitive decline.

Understanding the electrophysiological characteristics of SCD subjects is expected to receive great social support as it helps in early differential diagnosis and is a relatively low cost and non-invasive method. Therefore, the purpose of this study is to compare and analyze the power spectrum differences between SCD subjects and normal controls and use them as basic information for biomarker research that can diagnose early-stage AD in the future.

Materials and Methods

This study was conducted in accordance with the Declaration of Helsinki and approved by the institutional review board of

Chung-Ang University Hospital (IRB number 1802-004-16143). Written informed consent was obtained from all participants. The subjects of this study were 23 SCD patients (19 women and 4 men) and 23 normal control subjects (16 women) through medical record review of subjects who visited the memory impairment clinic at Chung-Ang University Hospital from January 1, 2014 to December 31, 2017 and 7 men were selected.

Evidence of brain disease, psychosis, epilepsy, or stroke on Magnetic Resonance Imaging (MRI) that is considered to cause cognitive impairment, drug addiction within the last 10 years, or history of alcoholism (drinking 3 or more a daily) were excluded. The selection criteria of the normal control group were suitable for the 28 normal elderly criteria of Christensen et al, and has a Korean Mini-Mental State Examination (K-MMSE) score of -1 SD (standard deviation) or higher, Korean-Instrumental Activities of Daily Living (K-IADL) was set to 0.42 or less, and Korean Dementia Screening Questionnaire (KDSQ) was set to 6 points or less.²¹⁻²³ the criteria for SCD subjects were complaining of memory impairment, but were less than -1 SD in the reference mean value considering age and education in all cognitive function areas of SNSB (Seoul Neuropsychological Screening Battery), and non-dementia state as a result of DSM-IV (diagnostic and statistical manual of mental disorder, 4th edition) by the American Psychiatric Association.²²⁻²⁷ SNSB is a test developed in Korea to comprehensively evaluate various cognitive functions. A comprehensive and in-depth assessment of cognitive functions such as attention, language and related function, visuospatial function, memory, and frontal/executive function will be conducted ([Supplementary Table 1](#)). All diagnoses were performed by a neurologist based on neuropsychological examination and criteria.²⁸

Resting-state EEG was conducted using the international standard 10–20 system (19 electrodes: Fp1, Fp2, F7, F3, Fz, F4, F8, T3, C3, Cz, C4, T4, T5, P3, Pz, P4, T6, O1, O2) and a digital electroencephalograph (Comet AS40 amplifier EEG GRASS; Telefactor, USA), and all electrodes were referred to linked ear references ([Supplementary Figure 1](#)).^{29,30} Electrode skin impedance was always below 5 k Ω . The EEG signal was analog-filtered with a band pass of 0.5–70 Hz and digitized and stored in magnetic disks for further analysis. EEG sampling was conducted for more than 15 minutes with eyes open for 30 s and

with eyes closed for 30 s, 10 times, at a rate of 200 Hz. While resting-state EEG data was recorded, patients were lying down in a resting position in a sound-attenuated room. EEG noise preprocessing and group analyses were conducted using iSyncBrain[®], v.1.0, 2018 (iMediSync Inc., Republic of Korea) (<https://isyncbrain.com/>), a cloud-based, artificial intelligence EEG analysis platform. The eyes-closed EEG segments were uploaded to iSyncBrain[®]. The EEG data uploaded by the user is automatically preprocessed and converted into a cleaned EEG from which noise has been removed by visual inspection and based on this, it generates key index values of QEEG and provides an analysis function between the selected comparison groups. In the detailed pre-processing process, band pass filtering is performed in the 1~45.5Hz section to check the delta-gamma region used for main EEG analysis, and a 60Hz notch filter is applied to additionally remove the noise from the power supply. After that, after applying the common average reference to remove the noise mixed throughout the measurement data, the process of removing the artifact components generated from the subject using bad epoch rejection and adaptive mixture independent component analysis (amICA) is performed to make clean EEG (Figure 1).^{31,32} At the sensor level, relative power at eight frequency bands (delta [1–3.99 Hz], theta [4–7.99 Hz], alpha1 [8–9.99 Hz], alpha2 [10–11.99 Hz], beta1 [12–14.99 Hz], beta2 [15–19.99 Hz], beta3 [20–29.99 Hz], and gamma [30–44.99 Hz]) was calculated using a power spectrum analysis. In the source-level analysis, the current distribution across the brain was assessed using the standardized low-resolution brain electromagnetic tomography technique,^{33,34} to compare relative power values in 64 regions of interests (ROIs) and the connectivity (the imaginary part of coherency) between ROIs.

Statistical Analysis

To compare demographic and cognitive assessment results between groups, Student's *t*-tests for continuous variables and Chi-square test for gender difference were performed with IBM SPSS version 25 (IBM, Armonk, NY, USA). Group analysis to compare the SCD and Normal groups was performed using the Kolmogorov–Smirnov test (KS) or the Shapiro–Wilk test (SW) for normality, and if normality was satisfied, an independent *t*-test was used. Statistical significance

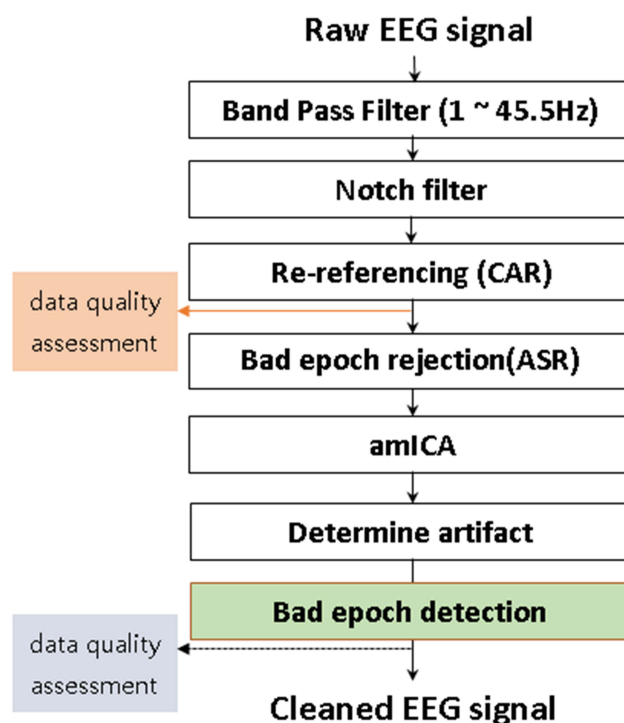


Figure 1 Pre-processing and artifact removal.

Abbreviations: CAR, common average reference; ASR, artifact subspace reconstruction.

was set at $p < 0.05$. All statistical processes for QEEG features were implanted in iSyncBrain[®] (iMediSync Inc., Seoul, Republic of Korea).

Results

The subjects of this study were 23 normal control subjects and 23 SCD subjects for a total of 46 subjects who satisfied the selection criteria. The average age of the normal control group was 72.02 ± 3.13 years old, 16 females and 7 males, and the average age of SCD group 72.14 ± 5.37 years, 19 females and 4 males. Demographic figures are presented in Table 1. In the sensor level of power spectral density (PSD) analysis, there was no statistically significant difference in all of the absolute power measured in 19 channels and the

Table 1 Demographic Characteristics

	Control (n = 23)	SCD (n = 23)	p value
Age (years)	72.02±3.13	72.14±5.37	0.923
Male/Female	7/16	4/19	0.300
Education (years)	7.65±2.40	7.30±3.88	0.717
MMSE	28.26±1.54	27.52±2.37	0.042

Abbreviations: MMSE, mini mental state examination; SCD, subjective cognitive decline.

Table 2 Relative Power of Delta Frequency According to 19 Electrode Channels

	Control (n = 23)	SCD (n = 23)	p value
Fp1	21.359±9.3962	25.158±12.4409	0.2489
Fp2	20.263±8.8501	27.021±11.1365	0.0276*
F7	22.982±8.0180	27.734±9.7246	0.0774
F3	15.777±6.8312	20.637±10.2570	0.0652
Fz	16.028±7.2617	18.692±10.2068	0.6925
F4	16.892±6.6713	21.682±8.7565	0.0428*
F8	21.845±7.8325	28.933±10.6835	0.0138*
T3	16.987±7.4356	18.672±6.9129	0.3229
C3	13.655±6.2337	16.728±6.9825	0.1227
CZ	15.666±7.5293	17.253±8.0339	0.4929
C4	14.091±5.3906	15.297±6.8044	0.5088
T4	15.931±7.1805	18.618±7.3864	0.2176
T5	13.155±8.3464	12.519±5.7746	0.7752
P3	13.210±6.2314	16.654±5.6658	0.0563
Pz	15.391±7.9076	17.514±6.7350	0.2443
P4	12.028±5.1138	13.565±5.1960	0.3174
T6	11.488±6.3242	10.861±5.4219	0.7252
O1	13.619±8.7554	14.803±8.5804	0.4290
O2	12.446±7.2015	12.998±6.5470	0.7868

Note: Unit, %; *p <0.05.

Abbreviation: SCD, subjective cognitive decline.

comparison analysis for each of the 8 bands were divided into 5 brain regions. In the relative PSD analysis, the average delta band power of the SCD group was significantly higher in Fp2, F4, and F8 than NC. In other channels, the average value of the SCD group was relatively higher than that of the normal control group, but it was not statistically significant (Table 2). The regional analysis showed that the delta band power in the frontal region was 0.24±0.09 of the SCD and 0.19±0.07 of the NC, which was significantly higher than in the SCD (p-value <0.05). The delta band in the other regions of the SCD group was higher, but not significant (Table 3). The topomap showed an overall increase in the bilateral frontal region of the delta band

Table 3 Relative Power of Delta Frequency Band According to the Brain Region

	Control (n = 23)	SCD (n = 23)	p value
Frontal	0.192±0.0667	0.241±0.0885	0.0396*
Central	0.144±0.0568	0.163±0.064	0.2878
Temporal	0.144±0.0643	0.151±0.0539	0.6786
Parietal	0.135±0.0594	0.158±0.0524	0.1688
Occipital	0.131±0.0769	0.139±0.0678	0.5828

Note: Unit, %; *p <0.05.

Abbreviation: SCD, subjective cognitive decline.

in the SCD group (Figure 2). There were no differences of the theta band power between the two groups in the channels and brain regions. Alpha1 band power of the O1 channel was 22.56±16.05 of the SCD group and 33.19±19.05 of the NC (p-value <0.05) (Table 4). Alpha 1 band of the occipital regions was 0.24±0.17 of the SCD and 0.33±0.19 of NC (p-value = 0.053) (Table 5). By topomap, an overall decrease in the occipital lobe region of the alpha 1 band was confirmed in the SCD group (Figure 3). There was no statistical difference in relative power of alpha2, beta1, beta2, and gamma band between the two groups in each channel and the entire brain region. Source-level analysis did not observe a statistically significant difference between the SCD and control groups for the source power of ROIs and the connectivity.

Discussion

In this study, we tried to find the difference in power spectrum between SCD subjects and community-based normal control groups, because SCDs showing normal performance in standardized neuropsychological tests have insufficient criteria or predetermined biomarkers for clinical or study purposes, and the electrophysiological characteristics of the SCD are not well known. We finally found an increase in slow wave delta waves in the frontal lobe and a decrease in the fast wave alpha 1 waves in the occipital lobe. SCD subjects showed a partial increase in delta waves in the frontal lobe region and a partial decrease in alpha1, a fast wave in the occipital region, compared to the NC. Quantitative studies to date have shown that AD slows EEG signaling as the disease progresses, and shows a significant decrease in the alpha band and an increase in the slow wave. Moreover, it has been shown that different frequency bands correlate the severity of cognitive impairment with the amount of power.³⁵ As can be seen from our results, we were able to confirm the difference between power spectrum changes due to aging and SCD when compared with community elders, and it was estimated that SCD exists in the MCI and AD extension lines.

These results are similar to previous studies showing increased slow waves and decreased fast waves in AD and MCI.^{36–38} The powers of the delta and theta waves were significantly higher than that of healthy subjects in the same age group.^{39,40} In recent studies, the increase in slow waves and decrease in fast

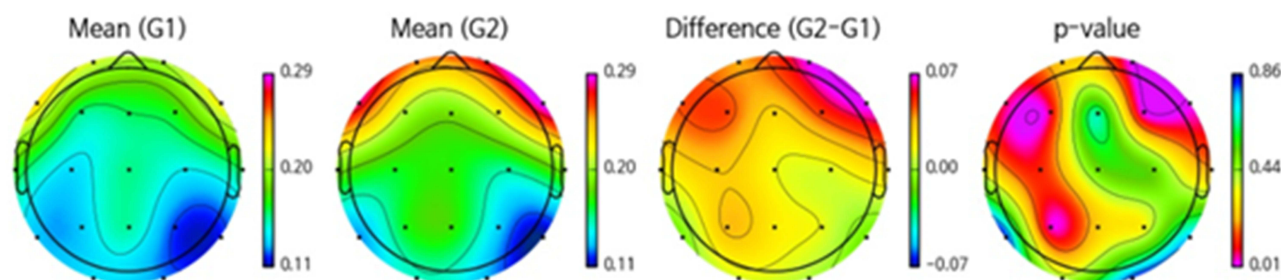


Figure 2 Topomap relative power - delta band (relative power differences between SCD (G2) and control (G1)).

Note: Unit: Percentage (%).

waves were suggested as the QEEG pattern of AD patients. In particular, an increase in theta waves and a decrease in the high-frequency band in the temporal lobe were remarkable. In recent studies, the increase in slow waves and decrease in fast waves were suggested as the power spectrum pattern of AD patients. In particular, an increase in theta waves and a decrease in the high-frequency band in the temporal lobe were remarkable.^{41–43} In one of the studies on AD related to the MMSE score, the lower the score, the higher the relative power of theta waves was found in the entire hemisphere.⁴⁴ In the MCI study, progressors' alpha

power decreased to the stable MCI group at a 1-year follow-up, and the decrease in alpha power was greater in the posterior lead of the MCI group.⁴⁵

SCD can be thought of as the preclinical stage of AD and the power spectral changes would be located on the spectrum of QEEG in MCI or AD, which showed different characteristics from community-based normal subjects in this study. However, there are very few power spectral change studies on the SCD group showing normal performance in all areas through an objective neuropsychological test. SNSB used for SCD diagnosis were standardized considering age and educational background, and normal categories were identified in five cognitive areas in our study and diagnosed by neurologists.

The power spectral changes of the SCD were similar to MCI and AD. However, a relative delta band power increased only in Fp2, F4, and F8, and relative alpha1 band power decreased only in the O1. Also, no statistically significant change in connectivity was found in the analysis at the source level. It is because SCD is considered to be one of the earlier stages of AD, and thought to be a compensable cognitive impairment with minor neuronal damage.⁴⁶

Our findings have some limitations to consider. SNSB, a standardized neuropsychological test tool used in our study, is a comprehensive neuropsychological test suite developed for the purpose of evaluating MCI and AD. It consists of various subtests for various cognitive functions, but due to the long test duration and somewhat burdensome test cost, the rate of cancellations by SCD subjects was high, which led to a lack of subjects and could have involved more severe SCD subjects who were worried about memory decline.

Table 4 Relative Power of Alpha I Frequency According to 19 Electrode Channels

	Control (n = 23)	SCD (n = 23)	p value
Fp1	1.087±16.2165	14.679±9.170	0.2443
Fp2	19.678±16.4521	15.600±10.9043	0.5679
F7	22.640±13.2559	16.215±6.9053	0.0826
F3	21.940±16.1500	16.415±12.2412	0.2720
Fz	25.932±17.3147	20.854±14.6744	0.3229
F4	20.640±16.0124	15.631±10.5715	0.3448
F8	20.470±13.3876	14.346±6.3087	0.1949
T3	22.524±10.6317	18.252±9.1895	0.1519
C3	19.428±12.9279	17.568±10.9322	0.6764
CZ	25.316±16.7857	22.778±13.1120	0.7252
C4	19.600±11.5888	16.421±9.8465	0.3448
T4	24.571±11.4873	19.827±11.9568	0.1770
T5	35.290±19.1073	28.581±17.4599	0.2205
P3	21.101±13.8604	14.785±7.8525	0.0950
Pz	25.606±17.2339	18.275±9.1799	0.2817
P4	25.471±16.6914	17.591±11.5220	0.0618
T6	38.081±19.0441	32.146±20.3525	0.3128
O1	33.192±19.0499	22.599±16.0474	0.0369*
O2	35.385±19.2938	26.941±19.8011	0.0907

Note: Unit, %; *p < 0.05.

Abbreviation: SCD, subjective cognitive decline.

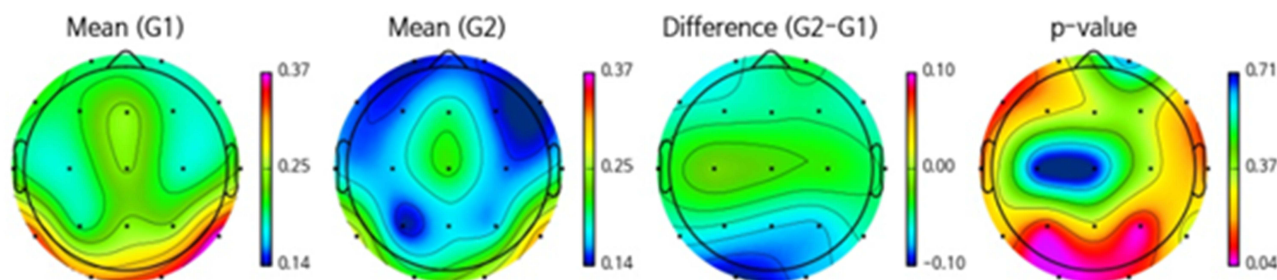


Figure 3 Topomap relative power - alpha I band (relative power differences between SCD (G2) and control (G1)).

Note: Unit: Percentage (%).

Although we were able to observe power spectral changes in SCD subjects in this cross-sectional study, longitudinal studies are needed to evaluate the predictability of future deterioration such as conversion to MCI.⁴⁷

Conclusion

Understanding the electrophysiological characteristics of SCD subjects is expected to receive great social support as it helps in early differential diagnosis while being a relatively low cost and non-invasive method. Therefore, the purpose of this study is to compare and analyze the power spectral change difference between SCD subjects and normal controls and use them as basic information for biomarker research that can diagnose early-stage AD in the future.

SCD subjects showed a partial increase of delta waves in the frontal lobe region and a partial decrease in alpha1, a fast wave in the occipital region, compared to the NC. SCD is considered one of the earliest clinical stages of AD and is predicted to be related to minor nerve damage. We were able to observe power spectral changes in SCD subjects in this cross-sectional study, a large number of subjects and longitudinal studies are needed to evaluate their predictability for future deterioration such as conversion to MCI.

Table 5 Relative Power of Alpha I Frequency Band According to the Brain Region

	Control (n = 23)	SCD (n = 23)	p value
Frontal	0.208±0.1443	0.155±0.0914	0.2533
Central	0.205±0.1270	0.180±0.1040	0.6134
Temporal	0.290±0.1388	0.238±0.1365	0.2030
Parietal	0.231±0.1466	0.161±0.0827	0.1241
Occipital	0.332±0.1848	0.239±0.1675	0.0532

Note: Unit, %.

Abbreviation: SCD, subjective cognitive decline.

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Disclosure

The authors report no conflicts of interest in this work.

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